



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁷ : H04R 25/00	A1	(11) International Publication Number: WO 00/70911 (43) International Publication Date: 23 November 2000 (23.11.00)						
<p>(21) International Application Number: PCT/US00/13276</p> <p>(22) International Filing Date: 15 May 2000 (15.05.00)</p> <p>(30) Priority Data:</p> <table border="0"> <tr> <td>09/311,156</td> <td>13 May 1999 (13.05.99)</td> <td>US</td> </tr> <tr> <td>60/203,983</td> <td>12 May 2000 (12.05.00)</td> <td>US</td> </tr> </table> <p>(71) Applicant (for all designated States except US): SOFTEAR TECHNOLOGIES, L.L.C. [US/US]; 175 Brookhollow Esplanade, Harahan, LA 70123 (US).</p> <p>(72) Inventors; and</p> <p>(75) Inventors/Applicants (for US only): JUNEAU, Roger, P. [US/US]; 134 Villere Drive, Destrehan, LA 70047 (US). CREEL, Lynn, P. [US/US]; 4449 Rue De La Harbor, Kenner, LA 70065 (US). DESPORTE, Edward, J. [US/US]; 1008 West 23rd Ave., Covington, LA 70433 (US). MAJOR, Michael [US/US]; 1656 Newport Pl., Apt. C, Kenner, LA 70065 (US). SIEGLE, Gregory, R. [US/US]; 4202 Platt, Kenner, LA 70065 (US). KINLER, Kelly, M. [US/US]; 171 Lakewood Drive, Luling, LA 70070 (US).</p> <p>(74) Agents: NEHRBASS, Seth, M. et al.; Garvey, Smith, Nehrbass & Doody, L.L.C., 3 Lakeway Center, Suite 3290, 3838 North Causeway Boulevard, Metairie, LA 70002 (US).</p>		09/311,156	13 May 1999 (13.05.99)	US	60/203,983	12 May 2000 (12.05.00)	US	<p>(81) Designated States: AE, AG, AL, AM, AT, AT (Utility model), AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, CZ (Utility model), DE, DE (Utility model), DK, DK (Utility model), DM, DZ, EE, EE (Utility model), ES, FI, FI (Utility model), GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KR (Utility model), KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SK (Utility model), SL, TJ, TM, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).</p> <p>Published <i>With international search report.</i></p>
09/311,156	13 May 1999 (13.05.99)	US						
60/203,983	12 May 2000 (12.05.00)	US						
<p>(54) Title: METHOD OF MANUFACTURING A SOFT HEARING AID</p> <p>(57) Abstract</p> <p>A hearing aid instrument (10, 70, 100, 132) of the in-the-ear type (and preferably CIC) provides a receptacle (18, 76, 112, 112A, 1115, 124) with electronic hearing aid components mounted thereto. The receptacle has a cavity for holding electronic components (e.g. battery, microphone, amplifier). A soft polymeric body (50, 94, 108) is preliminarily formed by encapsulating a plurality of the electronic hearing aid component shaped inserts (19, 35, 105). The body is soft and is shaped to conform to the ear canal of the user. After forming, the insert is removed to provide an insert cavity that can carry electronic components. The soft polymeric body (50, 94, 108) and encapsulated electronic hearing aid components (such as battery 90, battery door 89, amplifier 91, microphone 92 and locking tabs 93) define a soft structure compliant to the ear canal during use and that is substantially solid and free of void spaces between at least some of the components and the ear canal. This combination of soft compliant structure and encapsulated electronic hearing aid components addresses problems of peripheral leakage, poor fit, pivotal displacement that occurs with jaw motion and internal cross talk of components housed in prior art hollow type hearing aids.</p>								

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece			TR	Turkey
BG	Bulgaria	HU	Hungary	ML	Mali	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MN	Mongolia	UA	Ukraine
BR	Brazil	IL	Israel	MR	Mauritania	UG	Uganda
BY	Belarus	IS	Iceland	MW	Malawi	US	United States of America
CA	Canada	IT	Italy	MX	Mexico	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NE	Niger	VN	Viet Nam
CG	Congo	KE	Kenya	NL	Netherlands	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NO	Norway	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	NZ	New Zealand		
CM	Cameroon			PL	Poland		
CN	China	KR	Republic of Korea	PT	Portugal		
CU	Cuba	KZ	Kazakstan	RO	Romania		
CZ	Czech Republic	LC	Saint Lucia	RU	Russian Federation		
DE	Germany	LI	Liechtenstein	SD	Sudan		
DK	Denmark	LK	Sri Lanka	SE	Sweden		
EE	Estonia	LR	Liberia	SG	Singapore		

PATENT APPLICATION

TITLE OF THE INVENTION:

"METHOD OF MANUFACTURING A SOFT HEARING AID"

5 INVENTORS:

JUNEAU, Roger, P., a US citizen, of 134 Villere Drive, Destrehan, LA 70047, US;
CREEL, Lynn, P., a US citizen, of 4449 Rue de la Harbor, Kenner, LA 70065, US;
DESPORTE, Edward, J., a US citizen, of 1008 West 23rd Ave., Covington, LA 70433,
US;

10 MAJOR, Michael, a US citizen, of 1656 Newport Pl., Apt. C, Kenner, LA 70065, US;
SIEGLE, Gregory, R., a US citizen, of 4202 Platt, Kenner, LA 70065, US; and
KINLER, Kelly, M., a US citizen, of 171 Lakewood Drive, Luling, LA 70070, US.

ASSIGNEE

SOFTEAR TECHNOLOGIES, L.L.C., 175 Brookhollow Esplanade, Harahan, LA 70123,
15 US.

CROSS-REFERENCE TO RELATED APPLICATIONS

In the US, this is a continuation-in-part application of co-pending US patent application
Serial Nos. 09/181,539, 09/181,540, 09/181,541, 09/181,842, 09/181,843, 09/181,844 and
09/181,845, all filed 28 October 1998, which are continuations-in-part of application Serial No.
20 09/084,864, filed 26 May 26 1998, all incorporated herein by reference.

In the US, this is also a continuation-in-part of our co-pending US Patent Application
Serial No. 09/311,156, filed 13 May 1999, which is a continuation in part of co-pending US
Patent Application Serial No. 09/181,540 filed 28 October 1998, which is a continuation in part
of US Serial No. 09/084,864, filed 26 May 1998 (now US Patent 6,022,311). Each of these
25 patent applications and US Patent No. 6,022,311 are incorporated herein by reference.

Priority of our US Provisional Patent Application Serial No. 60/_____, filed 12 May
2000, Attorney Docket No. VP99128US (98029.4P9), entitled "METHOD OF
MANUFACTURING A SOFT HEARING AID", and incorporated herein by reference, is hereby
claimed.

30 Priority of our co-pending US Patent Application Serial No. 09/311,156, filed 13 May
1999, is hereby claimed.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

Not applicable

REFERENCE TO A "MICROFICHE APPENDIX"

Not applicable

5 BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention relates to hearing aids and more particularly to an improved hearing aid, its method of manufacture and an improved method of compensating for hearing loss. More particularly, the present invention provides an improved method and apparatus for compensating
10 for hearing loss that uses a construction combining a mounting receptacle (for example, a receptacle or modular face plate or semi-modular face plate) with a soft polymeric body that is joined to the mounting member and which encapsulates some of the electronic hearing aid components of the apparatus, the soft polymeric body being sized and shaped to conform to the user's ear canal during use. It may be possible to use a soft polymeric material as the receptacle
15 or face plate.

2. General Background of the Invention

The hearing industry has realized major strides in the development of high-fidelity, high-performance products, the most recent of which is digital signal processing technology. Hearing care professionals expected those advancements to solve the shortcomings of traditional
20 amplification, and to push the market forward. Those expectations have not been fully realized. While these developments have solved many of the problems associated with traditional electronic design and steadily gained market share, they have not fostered overall market growth.

The issues of early acoustic feedback, less than optimum fidelity and intermodulation of the frequency response cannot be completely resolved by electronic manipulation of the signal
25 by either analog or digital means.

Historically, custom-molded ear worn hearing instruments have been limited to an "acrylic pour" process as the means of the construction. With the advent of miniaturization and technological advancement of computer chip programming, the ear-worn instruments have become smaller and are positioned into the bony portion of the ear canal, commonly referred to
30 as "deep insertion technology".

Developments outside the hearing industry have culminated in a new level of micro-miniaturization of electronic components for industry applications. Consequently, advanced

signal processing can be housed in less space than was required for traditional electro-acoustic components.

With the development of programmable hearing aids, using either analog or digital signal processing, custom electronic design has shifted from the manufacturing level to the clinical level. The clinician can now customize the electro-acoustic response via software. It is no longer necessary for the device to be returned to the manufacturer for hardware changes to arrive at the desired electro-acoustic response. However, it is still often necessary to return the device for shell modifications.

In direct contrast to electronic advances within the industry, little or no advancement has been realized in custom prosthetic design. Since the late 1960's, when the custom in-the-ear hearing aid was developed, materials and construction techniques remained virtually unchanged. These materials and techniques were adopted from the dental industry, whereby the customized housing-commonly called a "shell" was constructed using acrylic of 90 point Durometer Hardness Shore D. This construction process provided the structure and the strength of material necessary to protect the electronics.

At the time the acrylic shell was developed, hearing instruments were worn in the relatively forgiving cartilaginous portion of the ear canal. Micro-miniaturization of electronic components, combined with increased consumer demand for a cosmetically acceptable device, has shifted the placement of the hearing aid toward the bony portion of the ear canal.

The bony portion of the canal is extremely sensitive and intolerant of an acrylic shell when that shell is over sized due to standard waxing procedures or is in contact with the canal wall beyond the second anatomical bend. Rigid acrylic that does not compress must pivot in reaction to jaw or head movement, thereby changing the direction of the receiver yielding a distorted acoustic response. In addition, the pivot action causes displacement of the device resulting in unwanted acoustic feedback. This problem has necessitated countless shell modifications, thereby compromising the precision approach of the original dental technology. Many such devices require some modification by the manufacturer. Most manufacturers can expect a high percentage of returns for modification or repair within the first year. Consequently, CIC (completely in canal) shell design has been reduced to more of a craft than a science. Although the recent introduction of the ultra-violet curing process has produced a stronger, thinner shell, the overall Shore Hardness remained unchanged.

The current trend for custom hearing aid placement is to position the instrument toward

the bony portion of the ear canal. The ear canal can be defined as the area extending from the concha to the tympanic membrane. It is important to note that the structure of this canal consists of elastic cartilage laterally, and porous bone medially. The cartilaginous portion constitutes the outer one third of the ear canal. The medial two-thirds of the ear canal is osseous or bony. The skin of the osseous canal, measuring only about 0.2 mm in thickness, is much thinner than that of the cartilaginous canal, which is 0.5 to 1 mm in thickness. The difference in thickness directly corresponds to the presence of apocrine (ceruminous) and sebaceous glands found only in the fibrocartilaginous area of the canal. Thus, this thin-skinned thinly-lined area of the bony canal is extremely sensitive to any hard foreign body, such as an acrylic hearing instrument.

Exacerbating the issue of placement of a hard foreign body into the osseous area of the ear canal is the ear canal's dynamic nature. It is geometrically altered by temporomandibular joint action and by changes in head position. This causes elliptical elongation (widening) of the ear canal. These alterations in canal shape vary widely from person to person. Canal motion makes it very difficult to achieve a comfortable, true acoustic seal with hard acrylic material. When the instrument is displaced by mandibular motion, a leakage or "slit leak" creates an open loop between the receiver and the microphone and relates directly to an electro-acoustic distortion commonly known as feedback. Peripheral acoustic leakage is a complex resonator made up of many transient resonant cavities. These cavities are transient because they change with jaw motion as a function of time, resulting in impedance changes in the ear canal. These transients compromise the electro-acoustic performance.

The properties of hard acrylic have limitations that require modification to the hard shell exterior to accommodate anatomical variants and the dynamic nature of the ear canal. The shell must be buffed and polished until comfort is acceptable. The peripheral acoustic leakage caused by these modifications results in acoustic feedback before sufficient amplification can be attained.

Hollow shells used in today's hearing aid designs create internal or mechanical feedback pathways unique to each device. The resulting feedback requires electronic modifications to "tweak" the product to a compromised performance or a "pseudo-perfection". With the industry's efforts to facilitate the fine-tuning of hearing instruments for desired acoustic performance, programmable devices were developed. The intent was to reduce the degree of compromise, but by their improved frequency spectrum the incidence of feedback was heightened. As a result, the industry still falls well short of an audiological optimum.

A few manufacturers have attempted all-soft, hollow shells as alternatives to acrylic, hollow shells. Unfortunately, soft vinyl materials shrink, discolor, and harden after a relatively short period of wear. Polyurethane has proven to provide a better acoustic seal than polyvinyl, but has an even shorter wear life (approximately three months). Silicones have a long wear life but are difficult to bond with plastics such as acrylic, a necessary process for the construction of custom hearing instruments. To date, acrylic has proven to be the only material with long term structural integrity. The fact remains, however, that the entire ear is a dynamic acoustic environment and is ill-served by a rigid material such as acrylic. Also, the acrylic hearing aids typically need to be returned to the manufacturer for major shell modifications.

10 The following references are all incorporated herein by reference:

U.S. Patent Nos.: 4,051,330; 4,375,016; 4,607,720; 4,716,985; 4,811,402; 4,870,688; 4,880,076; 4,937,876; 5,002,151; 5,068,902; 5,185,802; 5,201,007; 5,259,032; 5,530,763; 5,430,801; 5,500,902; and 5,659,621.

Also of interest and incorporated herein by reference are published Japanese patent application no. JA61-238198, the articles from December 1997 Journal of American Academy of Audiology, and Staab, Wayne J. and Barry Finlay, "A fitting rationale for deep fitting canal hearing instruments", Hearing Instruments, Vol. 42, No. 1, 1991, pp. 7-10, 48.

BRIEF SUMMARY OF THE INVENTION

The present invention provides a method of constructing a hearing aid and a soft hearing instrument that is solid (i.e. eliminates void spaces). This instrument includes a soft body portion that is truly soft, comprising an elastomer of about 3 to 55 Durometer Shore A and preferably 10-35 Durometer Shore A. This product is unique in that it is solid, with the electronic components actually encapsulated or embedded within the soft fill material. The fill material can be a Dow Corning® MDX-4-4210 silicone or a silicone polymer distributed by Factor II, Inc. of Lakeside, Arizona, designated as product name 588A, 588B, 588V.

The present invention provides a method that can replace traditional acrylic shell construction. Unlike the shell construction process, the ear impression is not modified, built up, or waxed. With the elimination of these steps, a more faithful reproduction of the ear impression is accomplished. With the present invention, the manufacturer should be able to produce a hearing aid body which will not need to be returned as frequently for modification as with present hard acrylic hearing aid bodies.

The apparatus of the present invention is virtually impervious to the discoloration,

cracking, and hardening experienced with polyvinyls and polyurethanes.

The hearing aid of the present invention provides a greater range of gain before feedback occurs.

The outer surface of the body of the present invention is preferably non-absorbent and
5 virtually impervious to cerumen.

As used herein, "in-the-ear hearing aids" includes all hearing aids which have all of the electronics positioned in the ear, and thus includes hearing aid styles ranging from full concha to CIC (completely in the canal) hearing aid styles.

The preferred embodiment of the present invention shown in the drawings is a CIC
10 hearing aid style.

BRIEF DESCRIPTION OF THE DRAWINGS

For a further understanding of the nature, objects, and advantages of the present invention, reference should be had to the following detailed description, read in conjunction with the following drawings, wherein like reference numerals denote like elements and wherein:

15 Figure 1 is a fragmentary, perspective view of the preferred embodiment of the apparatus of the present invention showing the mounting member portion thereof;

Figure 2 is an elevational view of the insert portion of the preferred embodiment of the apparatus of the present invention;

Figure 3 is an elevational side view of the insert portion of Figure 2, taken along lines 3-3
20 of Figure 2;

Figure 4 is a fragmentary, perspective view of a portion of the insert in Figures 2 and 3;

Figure 5 is a fragmentary, perspective view illustrating a portion of the insert of Figures
2 and 3;

Figure 6 is a fragmentary, elevational view of the preferred embodiment of the apparatus
25 of the present invention illustrating the mounting member and insert portions thereof;

Figures 7 and 8 are schematic views illustrating the method of the present invention;

Figures 9 and 10 are additional schematic, perspective views illustrating the method of
the present invention;

Figures 11 and 12 are perspective views illustrating the final method steps of the method
30 of the present invention including the assembly of electronic components to the soft elastomer body;

Figure 13 is a perspective, exploded view of a second embodiment of the apparatus of the present invention;

Figure 14 is a perspective view of the second embodiment of the apparatus of the present invention shown prior to the addition of liquid polymeric or elastomeric material to the cavity;

5 Figures 15-17 are perspective, schematic views illustrating the method of the present invention;

Figure 17 is a perspective view of the preferred embodiment of the apparatus of the present invention;

10 Figure 18 is a fragmentary perspective view of a third embodiment of the apparatus of the present invention showing the mounting plate portion of the mounting member;

Figure 19 is a perspective, fragmentary view of the third embodiment of the apparatus of the present invention illustrating one of the insert portion thereof;

Figure 20-20A are fragmentary perspective views of the third embodiment of the apparatus of the present invention showing the receptacle portion of the mounting member;

15 Figure 21-21A are partial, sectional, fragmentary views of the receptacle of Figure 20;

Figure 22 is a fragmentary, perspective view of the third embodiment of the apparatus of the present invention illustrative the mounting member including mounting plate and receptacle portions thereof and the insert portion thereof;

20 Figure 23 is a fragmentary, perspective view of the third embodiment of the apparatus of the present invention illustrating the mounting member and insert portions thereof;

Figure 24 is a fragmentary, perspective, exploded view of the third embodiment of the apparatus of the present invention illustrating the mounting member and insert portions thereof;

25 Figure 25 is a side elevational view of the third embodiment of the apparatus of the present invention illustrating the method step of attaching the shell having a mold cavity to the mounting member and insert portions;

Figures 26 and 27 are perspective views illustrating method steps of the present invention including the filling of the mold cavity with elastomeric material to encapsulate the inserts and support the mounting members;

30 Figure 28 is a perspective view of the third embodiment of the apparatus of the present invention illustrating the step of removing the shell from the soft polymeric bodies and the removal of the insert portions;

Figure 29 is a perspective view of the method of constructing the third embodiment of

the apparatus of the present invention showing the step of inserting the electronic hearing aid components into the soft polymeric body and mounting members;

Figure 30 is a perspective view of the third embodiment of the apparatus of the present invention;

5 Figure 31 is a partial perspective view of the method of constructing the fourth embodiment of the apparatus of the present invention showing the step of coating the vent tube with a bonding enhancer;

10 Figure 32 is a perspective view of the method of constructing the fourth embodiment of the apparatus of the present invention showing the step of removing the mold cavity from the mounting member and cured plastic polymeric body and removal of the hearing aid component assembly insert;

Figures 33-35 are perspective views of the method of constructing the fourth embodiment of the apparatus of the present invention showing the step of inserting the hearing aid component assembly into the soft polymeric body; and

15 Figure 36 is a partial perspective view of the method of constructing the fourth embodiment of the apparatus of the present invention showing the step of applying adhesive to the interface of the vent tube and mounting member.

DETAILED DESCRIPTION OF THE INVENTION

20 In Figures 1-12, there can be seen a method for constructing a hearing aid apparatus that is culminated in the addition of electronic components to the hearing aid apparatus as shown in Figures 11 and 12. Figure 12 shows the completed hearing aid apparatus designated generally by the numeral 10.

25 Hearing aid apparatus 10 is constructed with a beginning modular face plate 11 having a surface 12 and an opposing surface 13. A plurality of stacking pins 14 can be provided at the periphery 16 of modular face plate 11. Pins 14 enable shipments of several stacked modular face plates 11 with electronic components being placed there between.

30 A central opening 15 receives insert 19 during construction using the method of the present invention. The modular face plate 11 also becomes a part of the apparatus 10 of the present invention after construction is completed wherein the central opening 15 receives an electronic component carrying receptacle 18. Modular face plate 11 has an opening 17 that receives an end portion of a vent tube as will be described more fully hereinafter.

The combination of modular face plate 11 and insert 19 are used to form a soft

elastomeric or polymeric (e.g. silicone) body 50 that will carry electronic hearing aid components to define a hearing aid electronics package during use. The insert 19 is best seen in Figures 2-5. The insert 19 and face plate 11 are used to construct soft elastomeric or polymeric body 50 as shown in Figures 6-10.

5 In Figures 2-5, insert 19 includes an insert body 20 having a curved surface 21, a pair of opposed semi-circular flat surfaces 22, 23, and flat surface 24. Insert body 20 includes a cylindrical bore 25 that enables insert body 20 to be mounted on elongated, coated (with e.g. Teflon® brand PTFE) wire 27. Insert body 20 also provides an extraction handle 26 that aids in its removal from soft polymeric body 50 after molding is complete and the soft elastomeric body
10 has set.

In Figures 2-4, insert 19 also includes a receiver replica insert portion 28 having open ended bore 29. The open ended bore 29 enables the receiver replica insert 28 to be mounted on coated wire 27, as shown in Figures 2 and 3.

Each of the insert portions 20 and 28 can be adjustably, slidably mounted upon coated
15 (e.g. Teflon®) wire 27, as indicated schematically by the arrows 30, 31, in Figure 2. This feature enables a desired spacing between insert 20 and insert 28 to be achieved prior to construction of the soft polymeric body 50. It should be understood that the insert members 20, 28 can be of different size and configuration. The insert 28 is typically a receiver replica insert that can be configured to duplicate the size and shape of any number of commercially available receivers or
20 custom receivers. Similarly, the insert 20 is an insert that is of the size and shape of a receptacle 18 that will carry a number of electronic hearing aid components such as, for example, a battery, microphone, amplifier, etc.

Insert body 20 can be provided with a plurality of tabs 32 that fit sockets 33 next to central opening 15 as shown in Figures 1 and 5. Tabs 32 enable the insert body 20 to form a snap
25 fit with modular face plate 11 at sockets 33 prior to the formation of soft polymeric body 50 using injected liquid elastomer (e.g. silicone). Figures 4 and 6 illustrate the attachment of insert 19 to modular face plate 11.

In Figure 7, mold 36 is shown being attached to modular face plate 11 as indicated by arrows 40. In Figure 7, vent tube replica insert 35 has been added to face plate 11 at opening 17.
30 In Figure 8, mold 36 has been attached to modular face plate 11 using a bonding material. The construction of mold 36 and its attachment to a mounting member such as modular face plate 11 is shown and described in more detail in prior co-pending patent application serial number

09/181,540, filed October 28, 1998, which is hereby incorporated herein by reference.

In Figures 7 and 8, mold 36 has an outer surface 37, a wall 38, and a cavity 39. Mold 36 can be vacuum formed using a male mold and vacuum forming a sheet of heated film that conforms to the wall mold. Such a method of forming female mold 36 can be seen in our co-
5 pending US Provisional Patent Application Serial No. 60/_____, filed 12 May 2000, Attorney Docket No. VP99128US (98029.4P9), entitled "METHOD OF MANUFACTURING A SOFT HEARING AID", and incorporated herein by reference. A plurality of ports 41-45 are provided through the wall 38 as shown in Figures 7 and 8. In Figures 9 and 10, syringe 46 is shown adding elastomeric liquid material 47 through needle 48 into cavity 39, as indicated by arrow 49 in
10 Figure 9. The addition of elastomer 47 to cavity 39 encapsulates insert 19 and vent tube replica insert 35.

After the elastomer 47 is allowed to set, the insert 19 and vent tube replica insert 35 can be removed as indicated in Figure 10. The insert 19 and vent tube replica insert 35 are shown gripped by a technician's finger 55 and thumb 56 and removed as indicated by arrow 54 from soft
15 polymeric body 50 and mold 36. By removing the inserts 19, 35, a vent tube cavity 52 and an electronics cavity 53 are provided in soft polymeric body 50. An electronics package of a number of electronic components can then be added to cavities 52, 53.

In Figures 11 and 12, additional method steps of the present invention are shown. In Figure 11, the soft polymeric body 50 is shown having an outer surface 51 after removal of mold
20 36 and after a trimming of modular face plate 11. The modular face plate 11 is trimmed so that it exactly fits the outside contour of outer surface 51 of soft polymeric body 50 as shown in Figures 11 and 12.

In Figure 11, the cavities 52, 53 that remain after removal of the inserts 19, 35 are replaced with electronic hearing aid components that enable the hearing aid 10 to function,
25 including the components that are added into the cavities 52, 53 as indicated by arrows 57 in Figure 11. The electronic components that occupy cavities 52, 53 include e.g. battery 59, battery door 58, amplifier 60, microphone 61, wire harness 63, receiver 64, receiver sound tube 65, and locking tabs 62 that interlock with sockets 33 of modular face plate 11.

The completed hearing aid apparatus 10 as shown in Figure 12 with all of the electronic
30 components in position, occupying the two cavities 52, 53. A vent tube 66 is a tube that extends the full length of soft polymeric body 50, forming a connection with opening 17 in modular face plate 11.

In Figures 13-17, a second embodiment of the apparatus of the present invention is shown, designated generally by the numeral 70. Hearing aid apparatus 70 is constructed using an alternate method. In Figures 13 and 14, the hearing aid apparatus 70 begins with mold 71 having an outer surface 72, a wall 73 and a cavity 74. A number of ports 75 are formed through wall 73. A receptacle 76 that will carry electronic hearing aid components is attached to the mold wall 73 using a plurality of radially extending struts 80 as shown in Figures 13 and 14.

The receptacle 76 includes a pair of flat walls 78, 79 and a curved wall 77. This construction provides a cavity 81 for holding a number of electronic hearing aid components. Opening 95 in receptacle 76 enables a wiring harness 84 to pass through cavity 81 and into mold cavity 74 as shown in Figures 13 and 14. The components that extend through opening 95 and are external to cavity 81 of receptacle 76 include a portion of wiring harness 84, receiver 82, and receiver sound tube 83. Opening 96 in curved wall 77 of receptacle 76 enables vent tube 86 to pass through receptacle 76 curved wall 77 so that it can communicate with cavity 81.

The components that are contained with cavity 81 of receptacle 76 include battery 90, battery door 89, amplifier 91, microphone 92, and locking tabs 93 that form a connection with sockets 97 that are on the flat peripheral surface 98 of receptacle 76. In Figure 13, the combination of the electronic components 82, 83, 84, 86, 89, 90, 91, 92 are attached to mold 71 in a temporary fashion using the radially extending struts as shown in Figures 13 and 14 and as indicated schematically by the arrow 85 in Figure 13.

In Figure 15, syringe 47 can be used to inject liquid polymeric or elastomeric material, such as silicone, through needle 48 into cavity 74 of mold 71. In this fashion, the cavity 74 is filled with soft polymeric or elastomeric material and encapsulates the electronic components that are below openings 95, 96. Additionally, the material injected through needle 48 surrounds receptacle 76, closely conforming to its curved wall 77 and flat walls 78, 79.

The interior cavity 81 of receptacle 76 is not filled with polymeric material so that the cavity 81 can be occupied by some of the electronic hearing aid components. This construction enables replacement of the electronic hearing aid components that are contained within the cavity 81 of receptacle 76 without intrusion into the soft polymeric body 94 that is formed when the elastomeric or polymeric material in 47 injected with syringe 46 is allowed to set.

In Figure 16, the radially extending struts 80 have been removed as indicated by arrows 87. Arrow 88 indicates the addition of electronic hearing aid components to the cavity 81, namely battery 90, battery door 89, amplifier 91, microphone 92 and locking tabs 93. The

completed hearing aid apparatus 70 is shown in Figure 17.

Figures 18-30 show a third embodiment of the apparatus of the present invention, designated generally by the numeral 100 in Figure 30. In Figures 18-27, there can be seen a mounting assembly that includes a mounting plate 99 and receptacle 112 (See Figures 20-21).

5 An alternate receptacle 112A is shown in Figures 20A and 21A. The mounting plate 99 and receptacle 112 are positioned close to each other as shown in Figures 24-30 upon assembly. Mounting plate 99 has a central opening 101 and a periphery 102. The mounting plate 99 can be generally flat, providing opposed flat surfaces 103, 104. Receptacle 112 defines a mounting assembly with mounting plate 99 that can receive an insert such as members 27 and 28 that were
10 described above with respect to the embodiment of Figures 1-12.

Insert 105 is similar to the insert of the embodiment of Figures 1-12, the difference being removal of tabs 32 (see Figure 5). The embodiment of Figures 18-30 uses a receptacle 115 that is closely positioned to the plate 99 as shown in Figures 24-30. Insert 105 thus provides surfaces 21, 22, 23 as the insert shown in Figure 5. The tabs 32 have been removed. The insert 105 has
15 a smooth, flat undersurface 106. Curved surface 21 fits a cavity 119 of receptacle 115 during construction using the method of the present invention.

In Figures 19-21, receptacle 112 is comprised of a pair of flanges 113, 114 and an external curved wall 115. An opening 116 is provided in curved wall 115. The flanges 13, 14 provide arc shaped edges 117 and straight edge portions 118, 119. Arrows 120 in Figure 22
20 illustrate the assembly of insert 105, mounting plate 99, and receptacle 112.

In Figures 20A and 21A, an alternate construction for the receptacle is shown as receptacle 124. Receptacle 124 has spaced apart semicircular walls 125, 126 that can be generally parallel to each other. External curved wall 127 spans between walls 125, 126. Opening 129 in receptacle 124 allows a wiring harness to pass there through. A cavity 128 is
25 formed by walls 125, 126, 127. Each wall 125, 126 has a straight edge portion indicated as 130, 131 respectively in Figures 20A, 20B. Cavity 128 receives some electronic hearing aid components, similar to the cavity 122 of receptacle 112 (see Figures 29-30).

In Figure 23, the insert 105, mounting plate 99, and receptacle plate 112 have been assembled in operating position before molding using shell 36. Figures 24-27 illustrate the
30 molding steps of forming a soft polymeric body 108 about inserts 105, 35. Mounting plate 99 has an opening 121 that receives vent tube insert 35. Insert 105 has a cylindrically shaped open ended channel 25 that receives coated wire 27. Arrow 123 in Figure 24 illustrates the assembly

of coated wire insert 27 to cylindrically shaped opening 25 of insert 105. Figure 25 shows the completed assembly of mounting plate 99, receptacle 112, insert 105, and insert 35. In Figure 25, shell 35 is shown being lowered in the direction of arrows 107 until it fits over the inserts 105, 35, and registers against the flat surface 103 of mounting plate 99 as shown in Figures 26 and 27. As with the embodiment of Figures 1-12, the inserts 105, 35 extend through openings in the shell 36 so that when the inserts 35, 105 are removed after the soft polymeric body 108 is formed, they will leave behind recesses to be occupied by electronic hearing aid components.

In Figure 27, needle 48 is shown injecting elastomeric material (e.g. silicone) as indicated by the arrows 49 to the mold cavity formed inside of shell 36. After the elastomeric material 47 in Figure 27 is allowed to set, shell 36 is removed as shown by arrows 124 in Figure 28. A user then removes the inserts 35, 105 using thumb and forefinger 55, 56 as shown in Figure 28. The arrow 54 in Figure 28 indicates schematically the removal of the inserts to leave behind cavities 109, 110. In Figure 29, a user or technician uses his or her thumb and finger 55, 56 to pull an electronic hearing aid package into the cavities 109, 110 in soft body 108. As with the embodiment of Figures 1-12, these components can include, for example battery door 58, battery 59, amplifier 60, microphone 61, wire harness 63, receiver 64, receiver sound tube 65, and vent tube 66.

In the embodiment of Figures 13-30, a technician can sever the wiring harness 84 after the electronic components that are contained within cavity 81 have been lifted upwardly to the position of Figure 16, enabling those components to be serviced, replaced, etc. If the components below openings 95, 96 need to be serviced, those can be removed by either cutting the soft polymeric body 94 or by carefully removing them through expansion of the cavity in which they are contained.

In Figures 31-36, a fourth embodiment of the apparatus of the present invention is shown, designated generally by the numeral 132 in Figures 33, 34 and 35. Hearing aid 132 is constructed using the method shown in Figures 31-36. In Figure 31, vent tube 133 is shown prior to attachment to mounting member (e.g. acrylic) 134. The mounting member 134 has an opening 135. It should be understood that the mounting member 134 can receive any of the molds 36, 71 shown in the embodiments of Figures 1-30.

An insert 136 includes several sections designed to simulate portions of a hearing aid component assembly 152. For example, the insert 136 can include a section 137 designed to simulate an electronic hearing aid component, namely a receiver. The insert section 138 is

designed to simulate a wiring harness. The insert section 139 is designed to simulate a battery compartment or battery receptacle.

Once the selected mold such as 36 is attached to mounting member 134, it can be filled with a polymeric material (preferably silicone), such as is shown in Figure 9. However, in the embodiment of Figures 31-36, vent tube 133 is first coated with a bonding agent 149 such as A330 available from Factor II of Lakeside, Arizona. The vent tube 133 is then placed inside the mold cavity 39. The mold 36 is then attached (bonded) to mounting member 134 as shown and described with respect to the embodiments of Figures 1-30 (see Figure 7). Once the polymeric material has cured inside mold cavity 39, the mold 36 can be removed as indicated schematically by arrow 151. A technician then removes insert 136 as indicated schematically by the arrow 140 in Figure 32. The insert 136 includes an insert section 137 that simulates a receiver, an insert section 138 that simulates a wiring harness and an insert section 139 that simulates a battery compartment or battery receptacle. However, other shapes can be used for insert 136 so that a cavity 141 of desired shape is achieved. Upon removal of the insert 136, a cavity 141 is left behind, the cavity being positioned next to vent tube 133 as shown in Figure 32.

The cavity 141 simulates the sections of the provided insert 136, including a cavity section 142 that simulates a receiver, a cavity section 143 that simulates a wiring harness and a cavity section 144 that simulates a battery case or receptacle.

The bonding enhancer 149 can be applied to vent tube 133 using a spray or brush 145 as shown in Figure 31 as indicated schematically by the arrow 146. Vent tube 133 thus has an outer surface 147 that becomes coated with the bonding enhancer or bonding agent 148. Vent tube 133 provides a bore 148 which is not coated with the bonding enhancer, as it remains open to vent air flow in between the patient's ear canal and the exterior of the ear canal and hearing aid 132.

The polymeric filler material 150 that is added to mold 36 cavity 39 forms a soft and solid body having the provided cavity 141 into which a hearing aid component assembly 152 can be inserted, as indicated schematically by arrows 157 in Figure 33. This hearing aid component assembly can include both electronic hearing aid components and other components. As an example, in Figure 33, the hearing aid component assembly 152 includes a receiver 153, wiring harness 155, and battery compartment 156 that includes other hearing aid components such as battery 159, a microphone, an amplifier, or other hearing aid components.

Figure 34 illustrates the completion of and insertion of hearing aid component assembly 152 into the cavity 141 that was formed after the polymeric material 150 had cured and set, and

after which the shaped insert 136 had been removed. In Figure 35, arrows 158 schematically indicate a severing of excess vent tube 133 material and the severance of excess material from receiver tube 163. The receiver tube 163 and vent tube 133 thus communicate with the patient's inner ear generally opposite mounting member 134 as shown in Figures 33-35. The vent tube 133
 5 also communicates with the exterior of the patient's ear via an opening 162 in mounting member 134 (see Figure 36). A connection 161 can be formed between vent tube 133 and mounting member 134 using a needle 160 to apply an adhesive (such as a glue commercially available under the trademark SUPERGLUE) or other connection material or structure, for example.

PARTS LIST

10 The following is a list of suitable parts and materials for the various elements of the preferred embodiment of the present invention.

	10	hearing aid apparatus
	11	modular face plate
	12	surface
15	13	surface
	14	stacking pin
	15	central opening
	16	periphery
	17	vent tube opening
20	18	receptacle
	19	insert
	20	insert body
	21	curved surface
	22	flat surface
25	23	flat surface
	24	flat surface
	25	cylindrical bore
	26	extraction handle
	27	elongated coated wire
30	28	receiver replica insert
	29	open ended bore
	30	arrow

	31	arrow
	32	tab
	33	socket
	34	arrow
5	35	vent tube replica insert
	36	mold
	37	outer surface
	38	wall
	39	cavity
10	40	arrow
	41	port
	42	port
	43	port
	44	port
15	45	port
	46	syringe
	47	elastomer
	48	needle
	49	arrow
20	50	soft elastomeric body
	51	outer surface
	52	vent tube cavity
	53	electronics cavity
	54	arrow
25	55	technicians finger
	56	technician's thumb
	57	arrow
	58	door
	59	battery
30	60	amplifier
	61	microphone
	62	locking tabs

	63	wire harness
	64	receiver
	65	receiver sound tube
	66	vent tube
5	70	hearing aid apparatus
	71	mold
	72	outer surface
	73	wall
	74	cavity
10	75	port
	76	receptacle
	77	curved wall
	78	flat wall
	79	flat wall
15	80	radially extending strut
	81	cavity
	82	receiver
	83	receiver sound tube
	84	wire harness
20	85	arrow
	86	vent tube
	87	arrow
	88	arrow
	89	door
25	90	battery
	91	amplifier
	92	microphone
	93	locking tabs
	94	soft polymeric body
30	95	opening
	96	opening
	97	socket

	98	flat peripheral surface
	99	mounting plate
	100	hearing aid apparatus
	101	opening
5	102	periphery
	103	surface
	104	surface
	105	insert
	106	surface
10	107	arrow
	108	soft elastomeric body
	109	vent tube cavity
	110	electronics cavity
	111	trimmed periphery
15	112	receptacle
	113	flange
	114	flange
	115	external wall
	116	opening
20	117	arc shaped edge
	118	straight edge
	119	straight edge
	120	arrows
	122	cavity
25	123	arrow
	124	receptacle
	125	semicircular wall
	126	semicircular wall
	127	external wall
30	128	cavity
	129	opening
	130	straight edge

	131	straight edge
	132	hearing aid
	133	vent tube (e.g., polycarbonate plastic or resin, preferably vent tube material from Oticon in Denmark, with characteristics of about 1mm-2mm internal diameter and wall thickness of about 2mm and a rigidity which will reduce torsional load on hearing aid 132)
5		
	134	mounting member
	135	opening
10	136	insert
	137	insert section
	138	insert section
	139	insert section
	140	arrow
15	141	cavity
	142	cavity section
	143	cavity section
	144	cavity section
	145	brush
20	146	arrow
	147	outer surface
	148	bore
	149	bonding agent
	150	filler material
25	151	arrow
	152	hearing aid component assembly
	153	receiver
	154	receiver tube
	155	wiring harness
30	156	battery compartment
	157	arrow
	158	arrow

	159	battery
	160	needle
	161	connection
	162	opening
5	163	receiver tube

The foregoing embodiments are presented by way of example only; the scope of the present invention is to be limited only by the following claims.

CLAIMS

1. A method of manufacturing a hearing aid comprising the steps of:
 - a) forming a hollow shell with a surface that approximates the shape of a patient's ear canal;
 - 5 b) providing a mounting member;
 - c) mounting an electronic hearing aid component insert to the mounting member that simulates the shape of one or more electronic hearing aid components;
 - d) placing the mounting member and insert in the hollow shell;
 - e) filling the shell with a soft polymeric material that substantially encapsulates the
 - 10 insert;
 - f) replacing the insert with one or more electronic hearing aid components; and
 - g) wherein in step "e" the combination of insert and fill material define a soft structure that is compliant to ear canal movement during use.
2. The method of claim 1 further comprising the step of eliminating substantially all
- 15 void space between the shell and the insert with the filling in step "f".
3. The method of claim 1 wherein step "c" comprises providing a mounting member includes a receptacle for holding an electronic hearing aid component.
4. The method of claim 1 wherein step "c" comprises providing a mounting member that is an acrylic member.
- 20 5. The method of claim 1 wherein in step "c" the mounting member has medial and lateral side portions.
6. The method of claim 5 wherein in step "d" some electronic hearing aid components are attached to the medial side portion of the mounting member.
7. The method of claim 1 wherein in steps "e", "f" and "g", filling includes
- 25 encapsulating at least a receiver shaped electronic hearing aid component insert.

8. The method of claim 1 wherein steps "e", "f" and "g" comprise filling the shell with a soft silicone material that substantially encapsulates at least one of the electronic component inserts.

9. The method of claim 1 wherein the mounting member is a receptacle with a cavity
5 and further comprising the step of placing a battery in the cavity.

10. The method of claim 9 wherein the mounting member includes a plate member and a separate receptacle member and further comprising the step of positioning the plate member and receptacle member next to each other.

11. The method of claim 1 further comprising the step of removing the insert and
10 replacing the insert with a plurality of electronic hearing aid components.

12. A method of manufacturing a hearing aid comprising the steps of:

- a) forming a hollow shell with an inside surface that defines a mold cavity that approximates the shape of the human ear canal;
- b) providing an electronic hearing aid component insert;
- 15 c) placing the insert within the mold cavity;
- d) filling the mold cavity with a soft polymeric material that substantially encapsulates the electronic component insert;
- e) allowing the soft polymeric fill material to cure;
- f) removing the insert to define a void space;
- 20 g) placing one or more electronic hearing aid components in the void space, wherein in steps "e" and "f" the combination of the electronic components and fill material define a soft structure that is compliant to ear canal movement during use.

13. The method of claim 12 further comprising the steps of making an impression of the user's ear canal to construct a form and using the form in step "a" to shape the inside surface
25 of the hollow shell.

14. The method of claim 12 further comprising the step of using a form to shape the

mold cavity.

15. The method of claim 12 wherein the shell and mounting members are temporarily joined prior to step "d".

16. The method of claim 12 wherein in step "d" at least a receiver shaped insert is
5 encapsulated.

17. The method of claim 12 wherein in step "d" at least a battery compartment insert and a receiver shaped insert are encapsulated.

18. The method of claim 12 wherein the mounting member is a battery compartment shaped insert.

10 19. The method of claim 12 wherein in step "b" the mounting member is of a hard plastic construction.

20. The method of claim 19 wherein the bonding layer includes multiple coatings applied to the mounting member.

15 21. The method of claim 12 wherein in step "b" the mounting member is a hard plastic and in step "e" the soft polymeric material includes silicone.

22. A method of manufacturing a hearing aid comprising the steps of:
a) making a mold with a mold cavity that includes an inside surface that closely approximates the shape of a patient's ear canal;
b) providing an insert that includes members having the size and shape of a number
20 of selected electronic hearing aid components;
c) placing the insert in the mold cavity;
d) filling the mold cavity with a liquid polymeric material that substantially encapsulates at a portion of the insert;
e) allowing the polymeric material to set;

- f) removing the insert to provide an insert cavity;
- g) replacing the insert with a hearing aid electronics package that fits the insert cavity;
- h) wherein the combination of polymeric material and electronics package define a soft hearing aid structure that is compliant to ear canal movement during use.

23. The method of claim 1, wherein the hearing aid is sized to fit completely in the ear canal of a user.

24. The method of claim 12, wherein the hearing aid is sized to fit completely in the ear canal of a user.

25. The method of claim 22, wherein the hearing aid is sized to fit completely in the ear canal of a user.

26. A hearing aid comprising:
- a) a soft body having an outer surface that approximates the shape of a patient's ear canal;
 - b) a socket in the soft body that is sized and shaped to closely conform to a hearing aid electronics package of a number of electronic components; and
 - c) an electronics package that fits the socket, the electronics package including a receptacle that has an interior cavity, at least some of the electronic components occupying the cavity.

27. The hearing aid of Claim 26 wherein some of the electronic components are positioned externally of the cavity.

28. The hearing aid of Claim 27 further comprising a wiring harness that extends from the cavity to an electronic component external to the cavity.

29. The hearing aid of Claim 26 wherein the hearing aid components positioned externally of the receptacle cavity include a receiver.

30. The hearing aid of Claim 26 wherein the walled receptacle has a cavity occupied by electronic components, an external wall, and wherein the soft body substantially conforms to the external wall.

31. The hearing aid of Claim 26 further comprising a wiring harness that connects the
5 receiver to an electronics component in the cavity.

32. The hearing aid of Claim 26 wherein the soft body has an inner surface that closely conforms to the electronics package.

33. The hearing aid of Claim 26 wherein the soft body is of a polymeric material

34. The hearing aid of Claim 26 wherein the receptacle includes a pair of mounting
10 members.

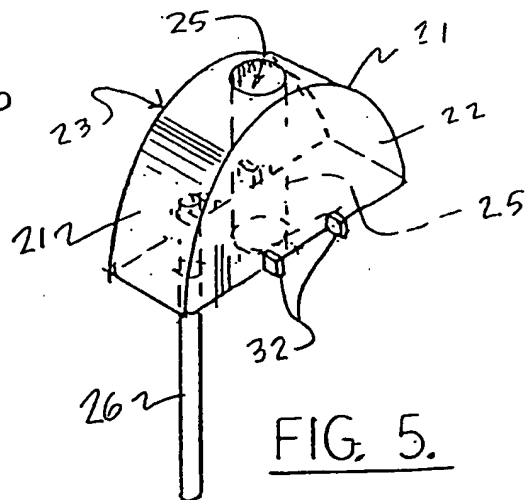
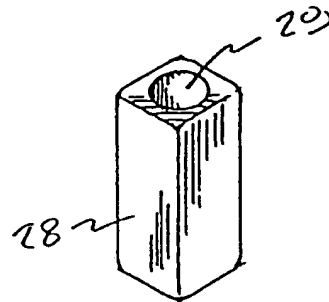
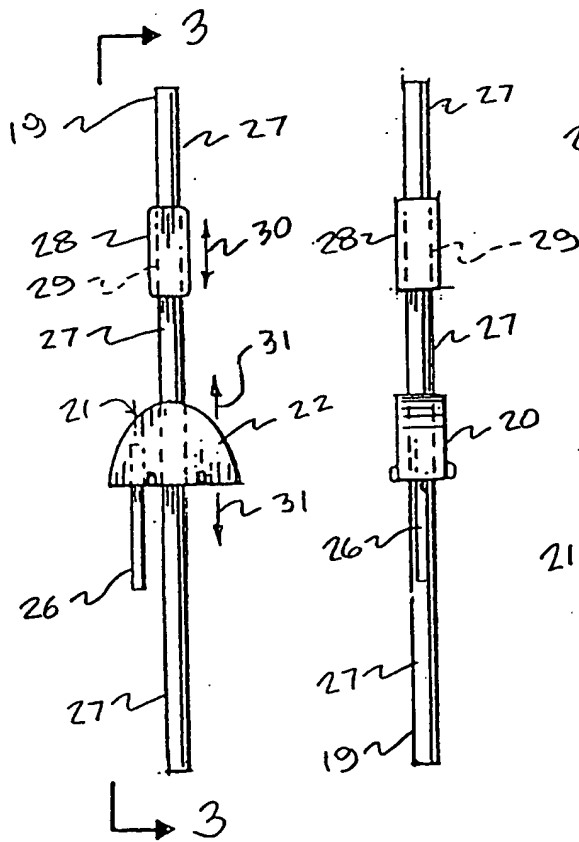
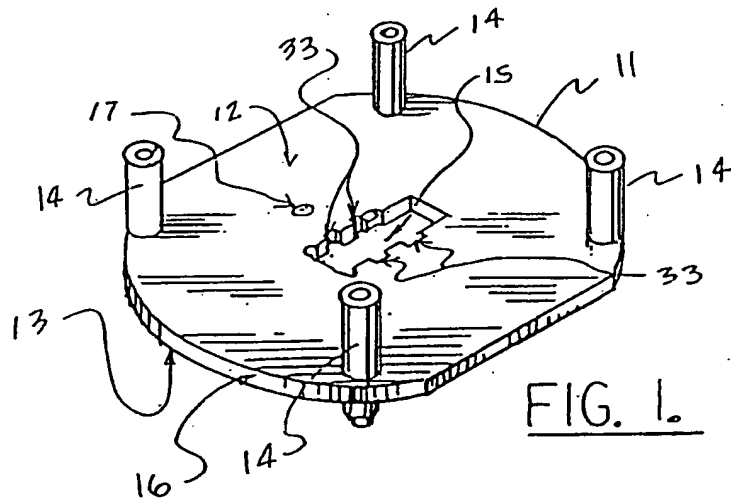
35. The hearing aid of Claim 34 wherein one of the mounting members is a mounting plate.

36. The hearing aid of Claim 34 wherein one of the mounting members has a socket that receives an electronic hearing aid component.
15

37. The hearing aid of Claim 34 wherein the mounting members are positioned next to each other.

38. The hearing aid of Claim 36 wherein one of the mounting members is supported by the soft body.

20 39. The invention substantially as shown and described herein.



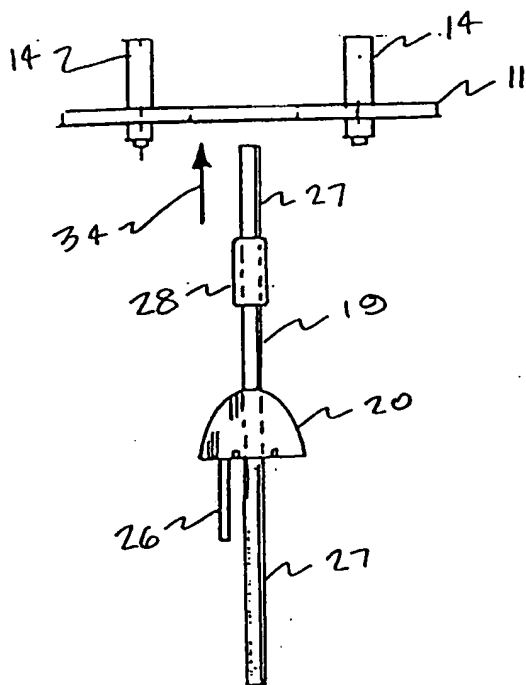


FIG. 6.

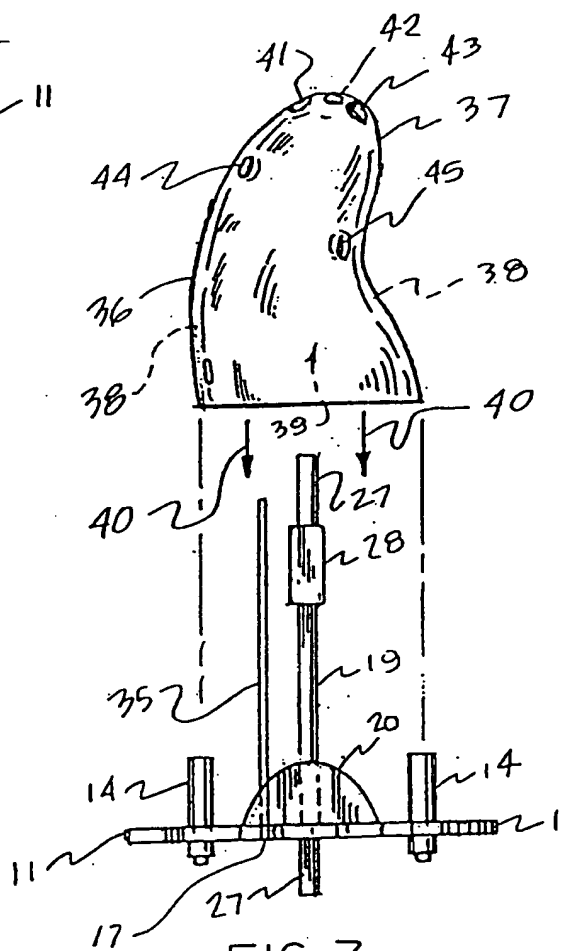


FIG. 7.

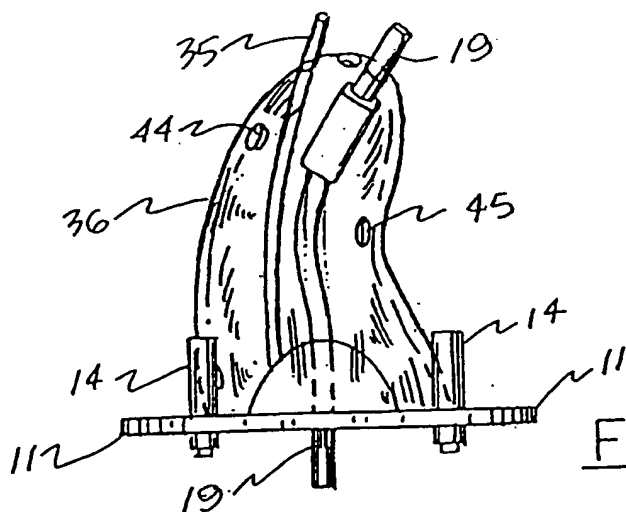
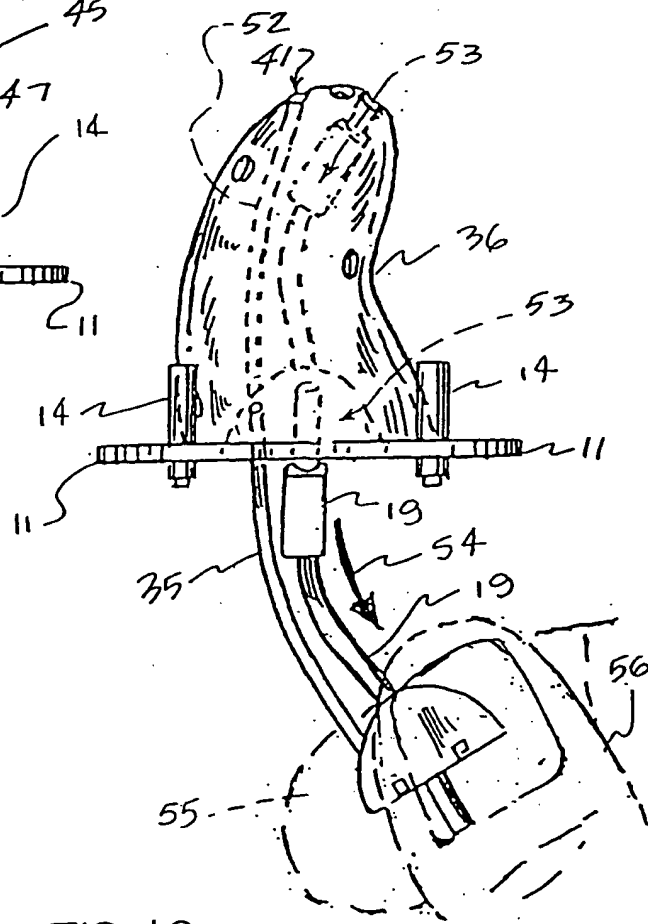
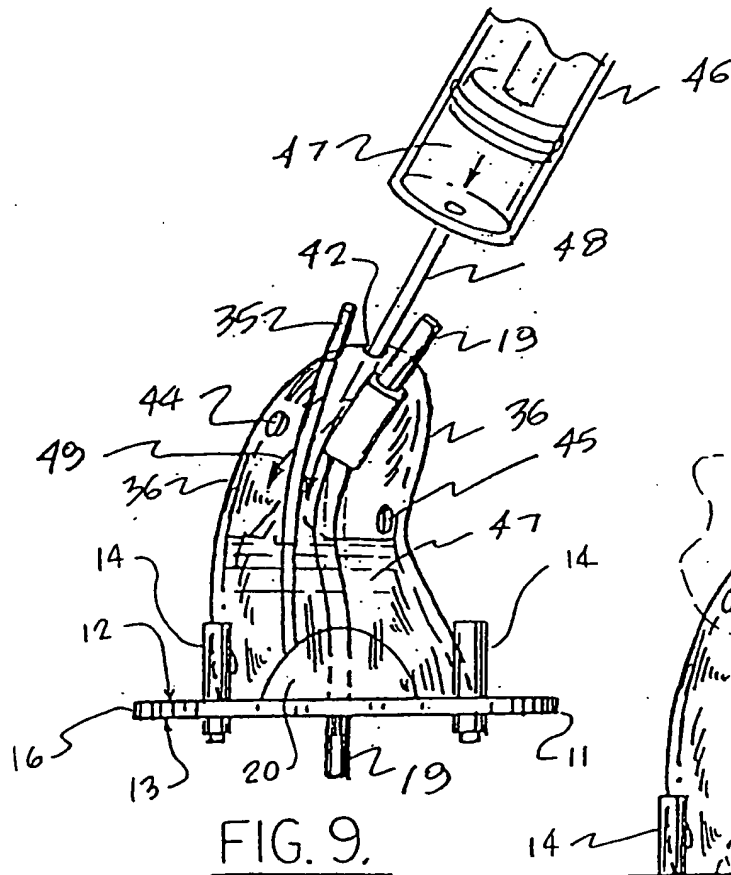
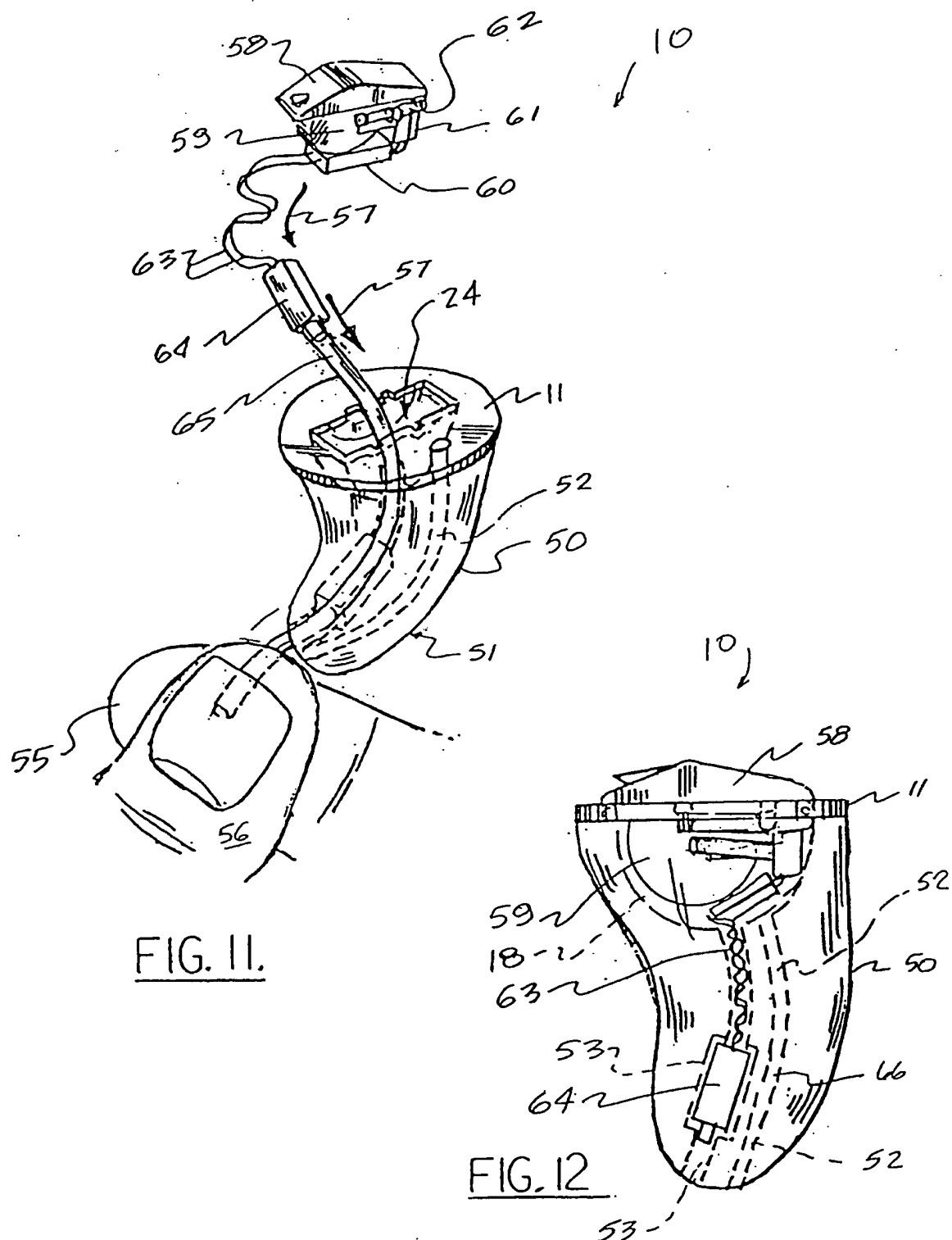
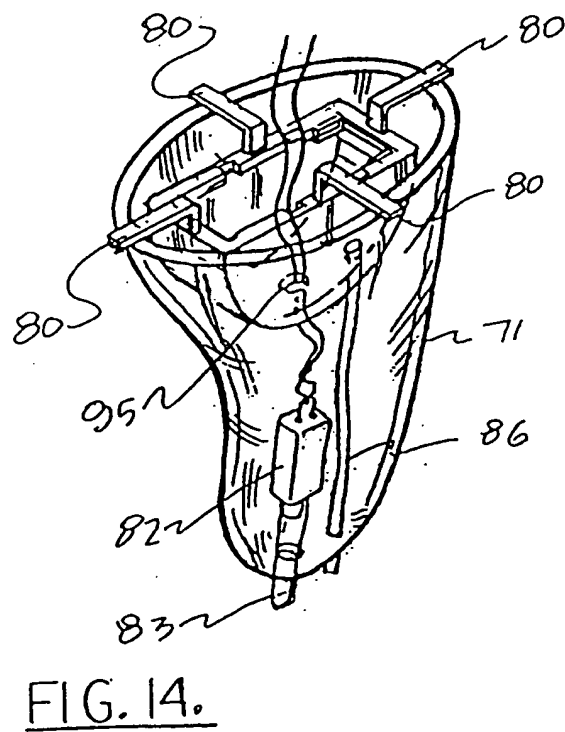
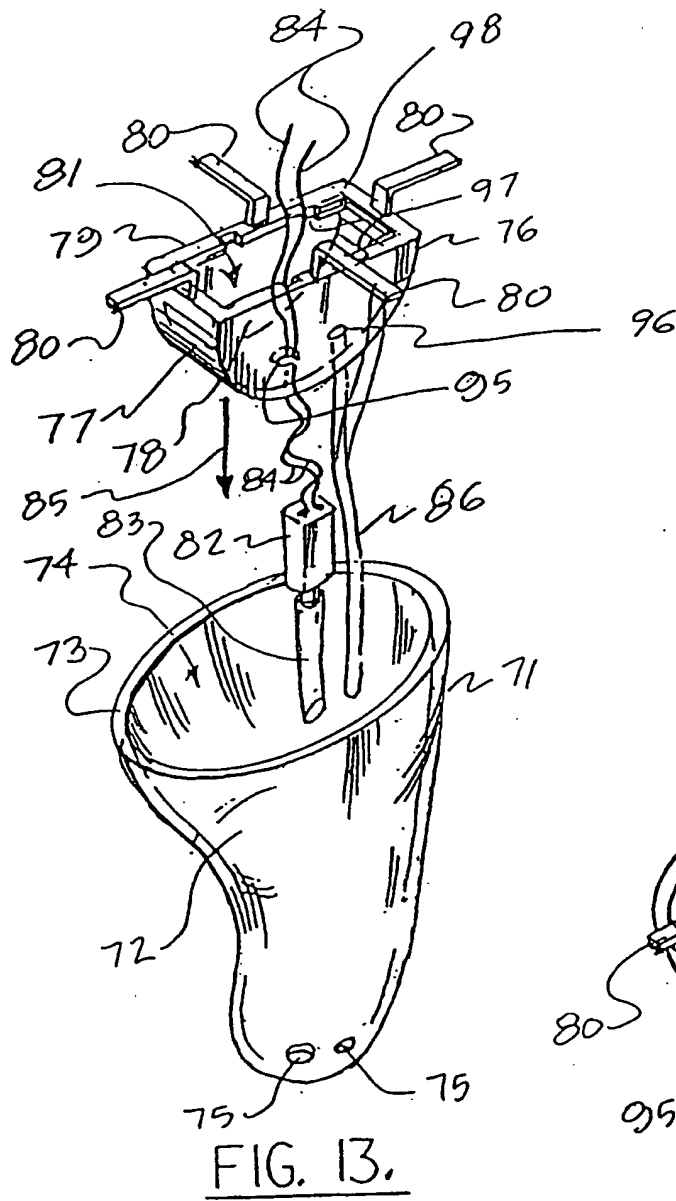


FIG. 8.







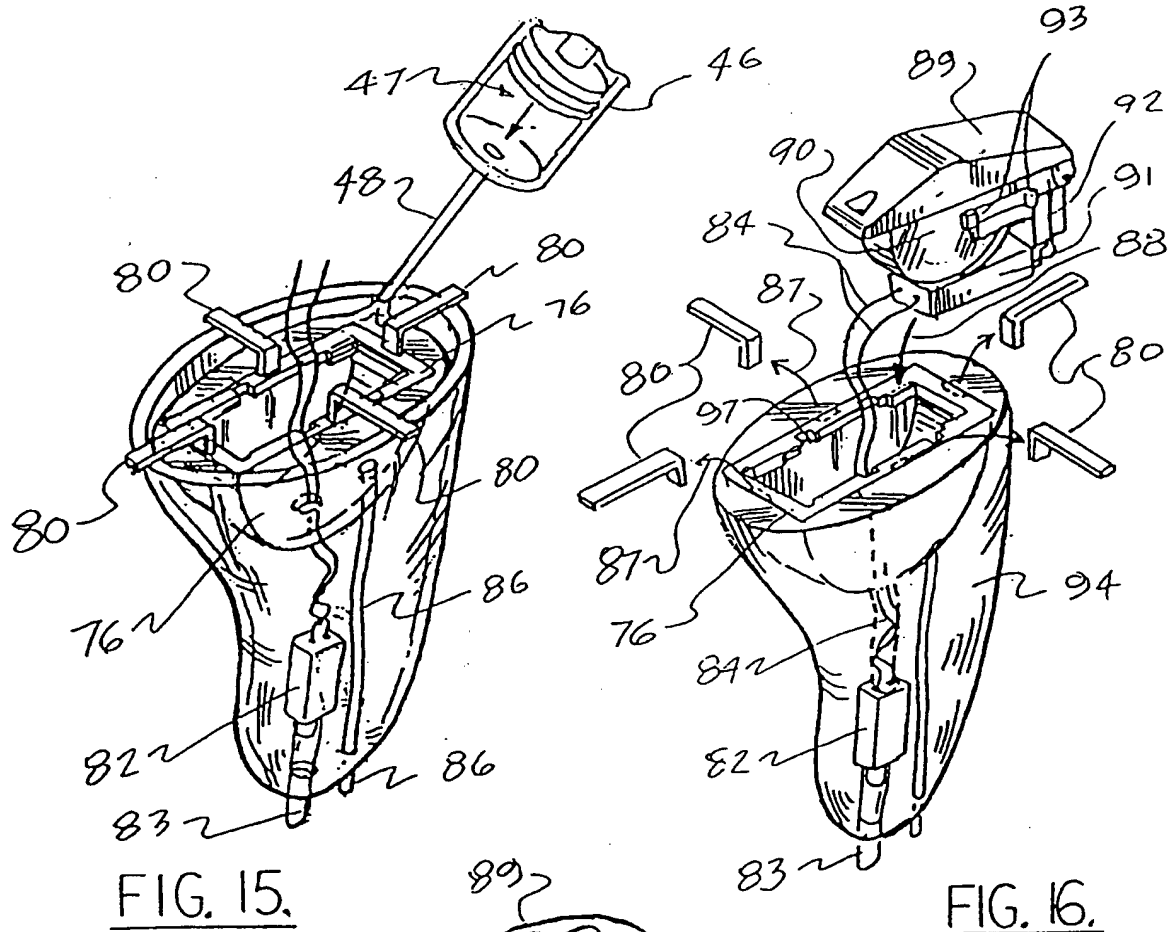


FIG. 15.

FIG. 16.

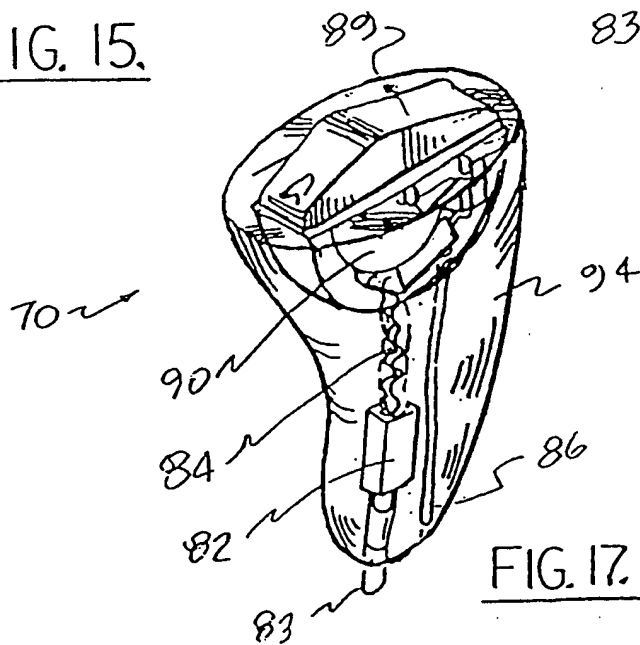


FIG. 17.

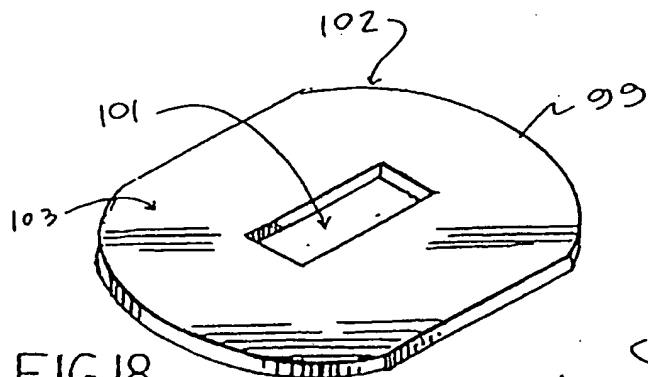


FIG. 18.

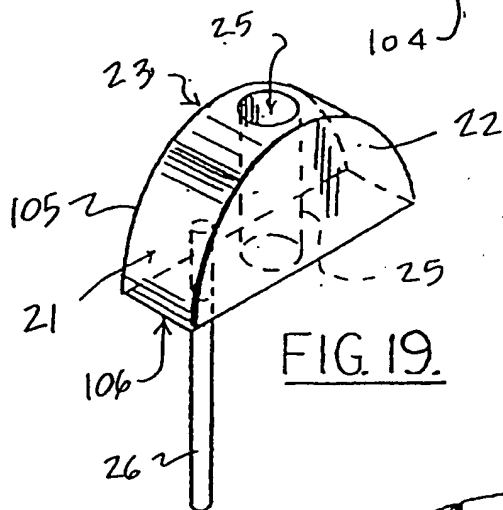


FIG. 19.

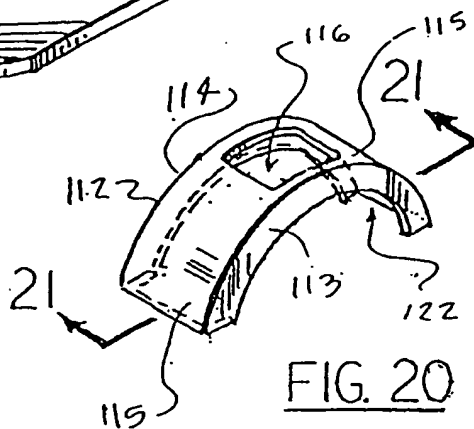


FIG. 20.

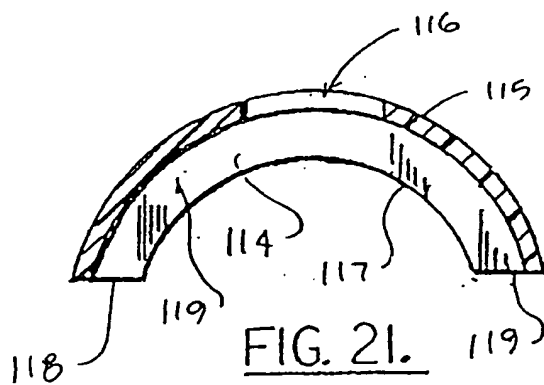
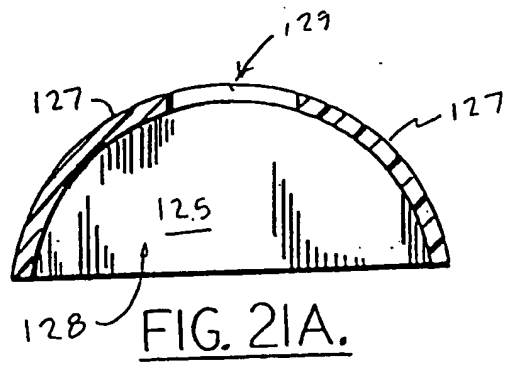
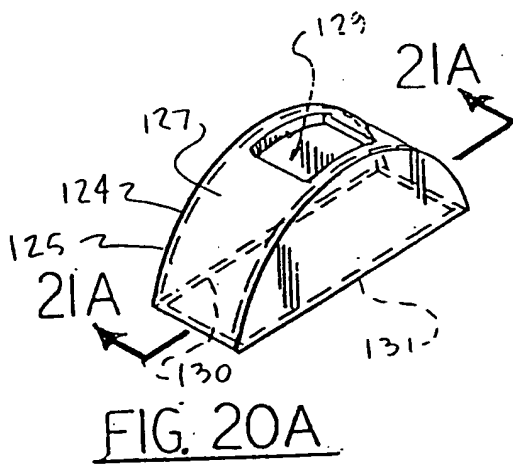
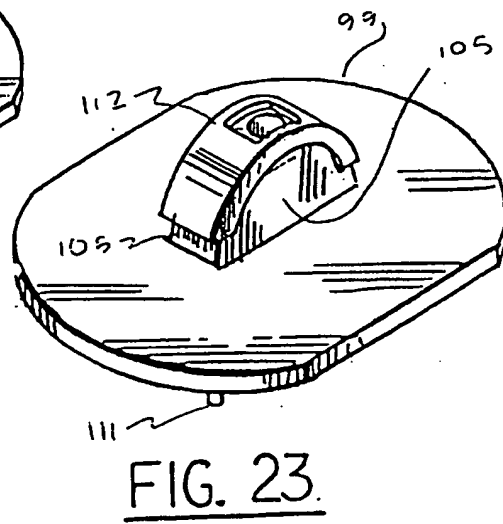
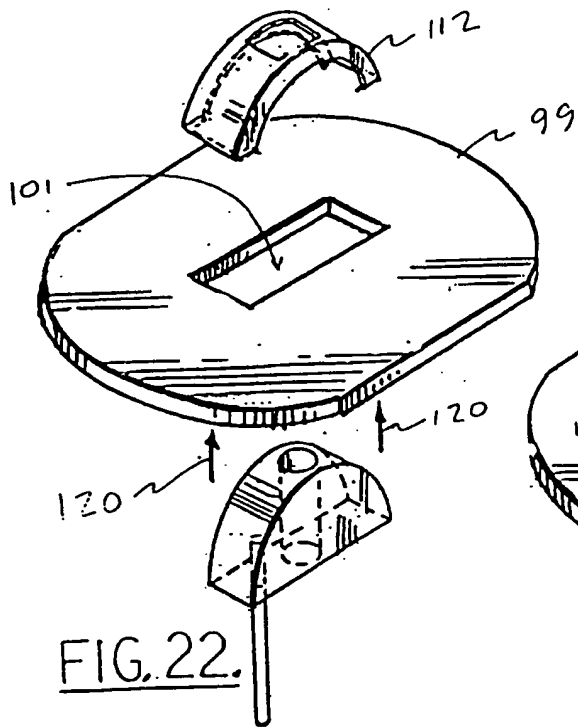


FIG. 21.



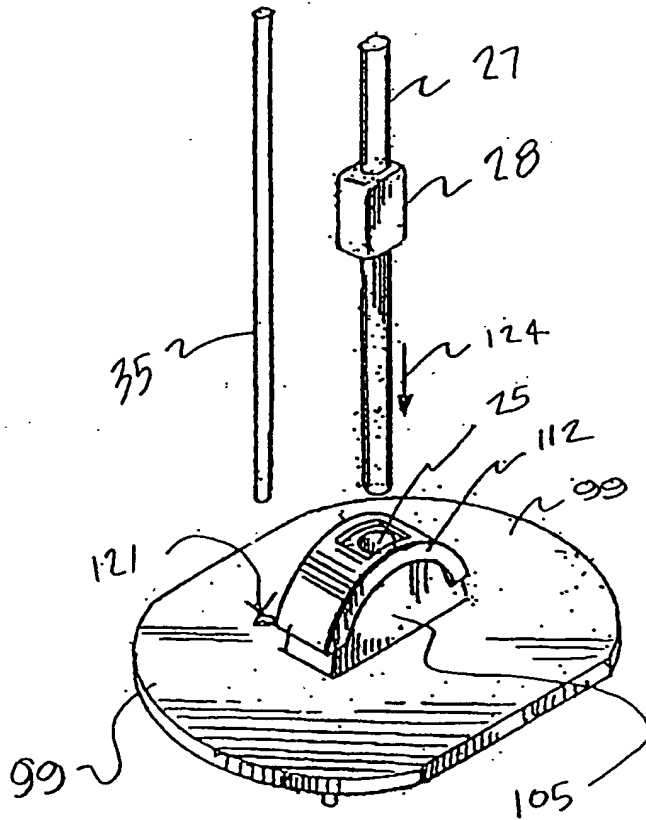


FIG. 24.

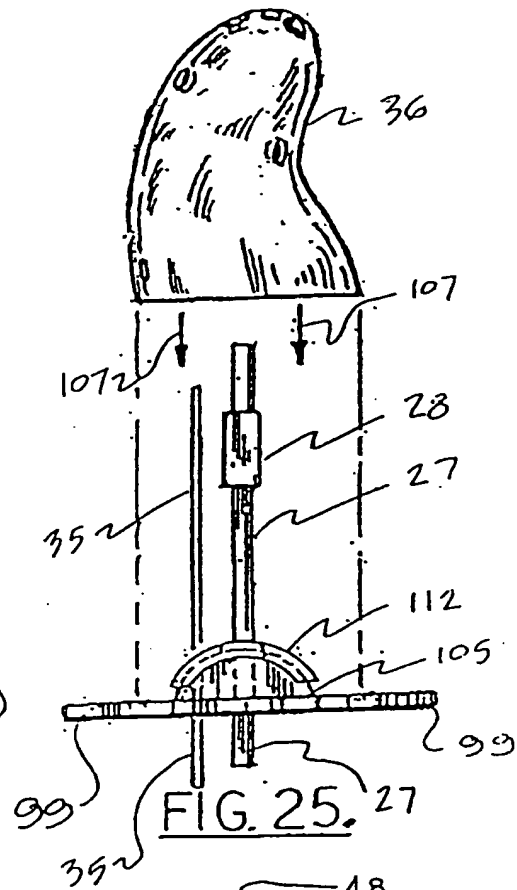


FIG. 25.

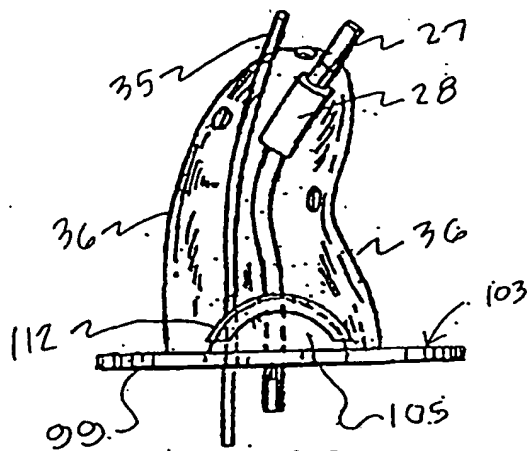


FIG. 26.

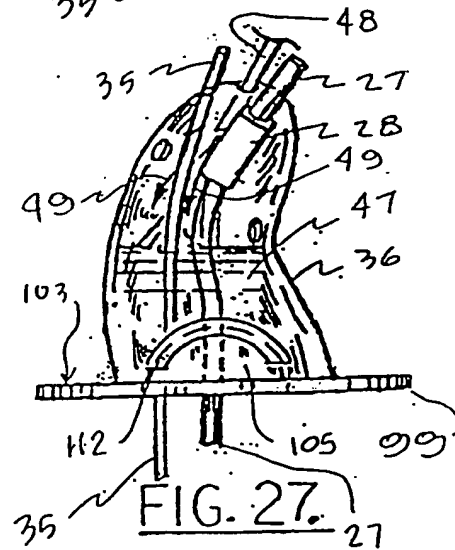


FIG. 27.

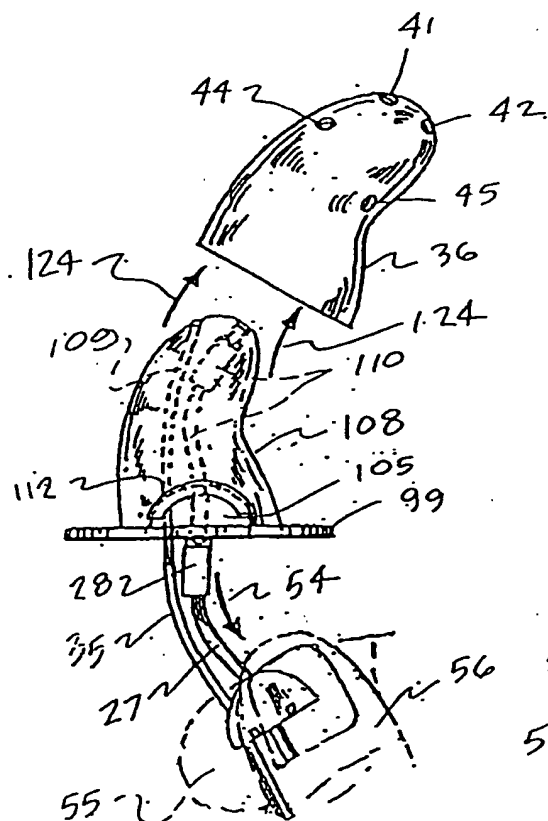


FIG. 28.

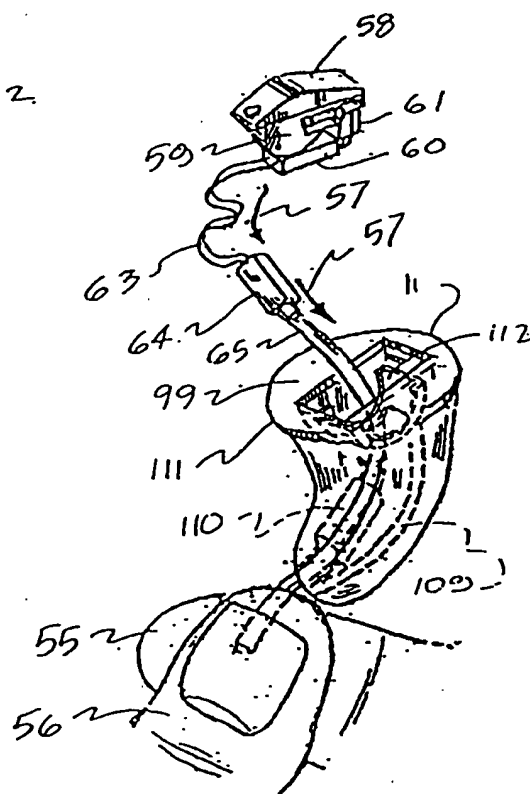


FIG. 29

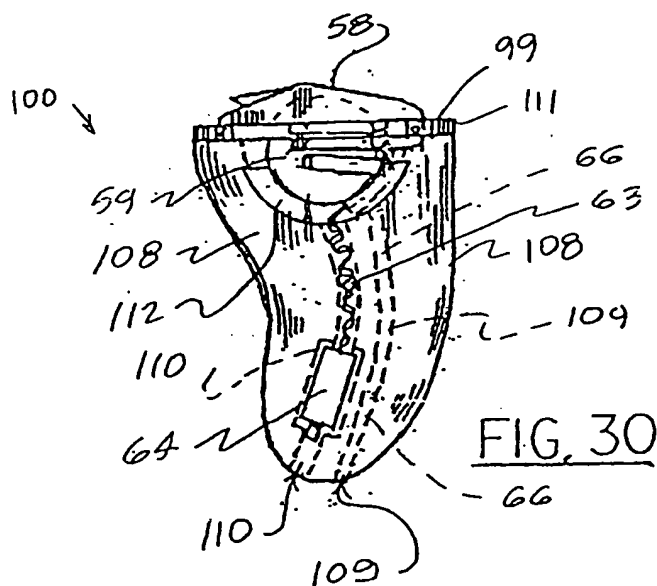
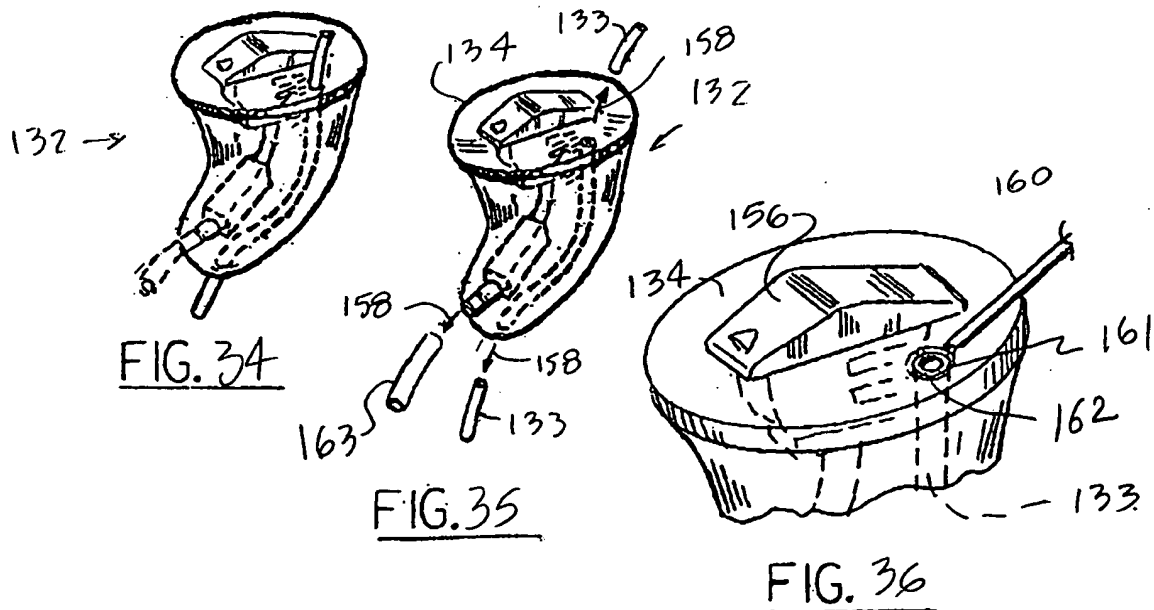
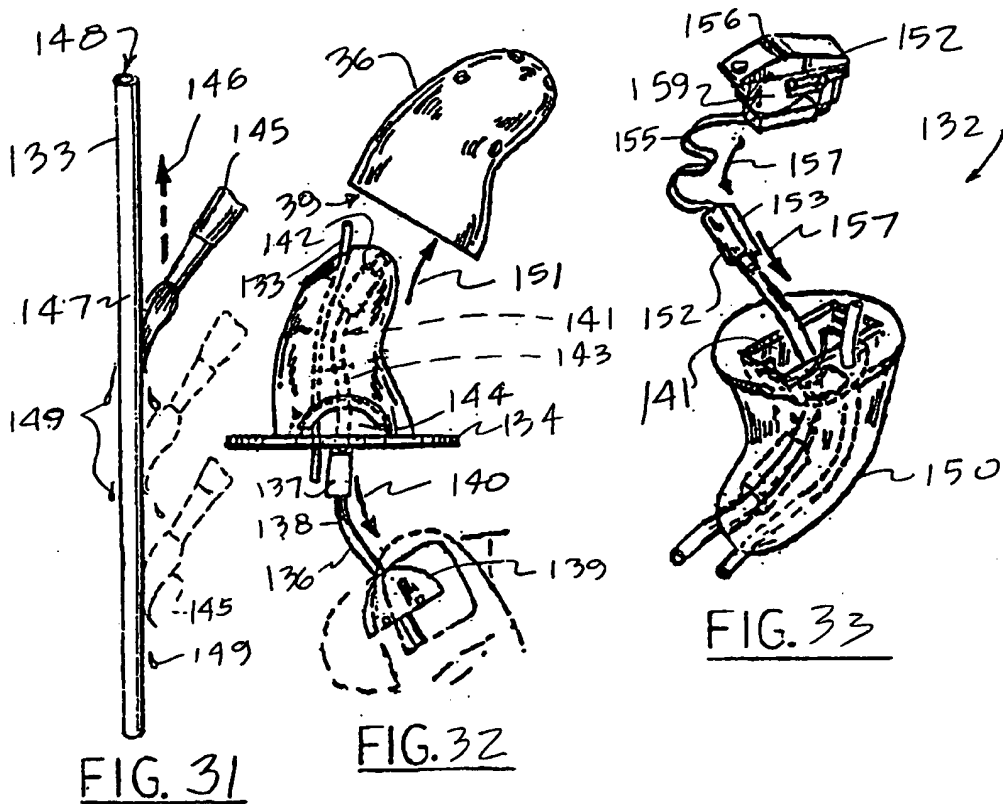


FIG. 30



INTERNATIONAL SEARCH REPORT

International application No.

PCT/US00/13276

A. CLASSIFICATION OF SUBJECT MATTER

IPC(7) :H04R 25/00

US CL :181/68-69.2; 600/025; 607/055-057

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 181/68-69.2; 600/025; 607/055-057

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X,P	US 6,022,311 A (JUNEAU et al.) 08 February 2000, entire document.	1-39
X	US 4,375,016 A (HARADA) 22 February 1983, entire document.	26-39

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"A" document defining the general state of the art which is not considered to be of particular relevance	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"E" earlier document published on or after the international filing date	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"&" document member of the same patent family
"O" document referring to an oral disclosure, use, exhibition or other means	
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

13 AUGUST 2000

Date of mailing of the international search report

30 AUG 2000

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
Box PCT
Washington, D.C. 20231

Facsimile No. (703) 305-3230

Authorized officer

JOHN LACYK

Telephone No. (703) 308-2995